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CO and CO-releasing molecules in medicinal chemistry

Since the discovery that CO acts as a cytoprotective and homeostatic molecule, increasing research efforts have been devoted to the exploitation of its therapeutic effects. Both endogenous and exogenous CO improves experimental lung, vascular and cardiac injuries and protects against several inflammatory states. The technology is now in place to bring CO to clinical applications, but the use of the gaseous molecule poses several problems. The challenges associated with the clinical implementation of the gas have in part been answered by the development of CO-releasing molecules (CO-RMs). As stable solid forms of CO, these molecules represent an alternative to the administration of carbon monoxide (orally or by injection). In this article, we present insights into the biochemical action of CO and discuss the efficacy of CO and CO-RMs in preclinical disease models. Recent advances in the CO-RMs field are critically addressed.

CO-releasing molecules (CO-RMs) are an emerging class of pharmaceutical compounds that are intended to specifically deliver CO to diseased or inflamed tissues in order to initiate and promote therapeutic effects at the site of disease. The potent beneficial action of CO-RMs is directly attributed to the biochemistry of the released CO. Healthy humans constantly produce CO. Available data indicate production of CO as approximately 10 cm³/d, but elevated levels are measured in patients suffering from various pathological conditions [1]. Endogenously, the formation of CO is due to a family of enzymes known as heme oxygenases (HOs) of which three isoforms have been identified: HO-1, -2 and -3 [2–4]. In our body HO-1 and -2 carry out the formation of CO via the oxidative metabolism of heme (**FIGURE 1**), while the function of HO-3 is still unknown. HO-1, mainly found in the spleen and the liver, is the only inducible isoform of this enzymatic family. It is ubiquitously expressed in all mammalian tissues. Mounting evidence indicates that increased cellular stress will result in a cascade of stimuli ultimately leading to the up-regulation of transcription of the enzyme [2–5]. HO-2 and -3 are constitutively expressed and they are mainly found in the brain and testes. Abnormality in the function of HO's and in metabolism of their action-derived CO have been linked to different diseases [2].

Despite the fact these enzymes have been known for over half a century, their action-derived CO was considered for decades as only a 'byproduct' of their metabolic reactions. Today

we know that the diatomic molecule plays a crucial role as a gasotransmitter, and when exogenously applied it mediates a therapeutic effect in different pathologies including cancer, neurodegenerations, hypertension, heart diseases, liver disfunctions, inflammation and infections. In medicine, CO applications have also advanced in the field of organ transplantation and preservation. Initially, the potential therapeutic effects of CO were demonstrated in a model of acute lung injury and subsequently, in a seminal paper by Otterbein and his group, it was demonstrated that CO is able to suppress the development of post-transplant arteriosclerotic lesions in rat recipients of allogenic aorta transplants [6]. Currently CO is evaluated in several clinical trials (Phase I–III). These include: improvement of cardiac injury after myocardial infarction (in conjunction with heme arginate, Phase I/II); anti-inflammatory effects in chronic obstructive pulmonary disease (Phase II completed); treatment of patients with intestinal paralysis after colon surgery (Phase II); prevention of lung inflammation (Phase I completed) [1]. The protective effects of CO as vasodilator (and probably biliverdin and bilirubin derived from the heme metabolic pathway) have also been successfully evaluated in several cardiovascular diseases including pulmonary arterial hypertension, for which there is no treatment.

Although the technology is now in place to bring CO to clinical applications [7], the use of the gaseous molecule poses several problems. First, the dose control of the gas is demanding. Inhaled gaseous CO causes direct cell

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Key Terms**CO-releasing molecules:**

Any compound capable of liberating CO under physiological conditions. The loss of CO may be either spontaneous (e.g., thermal activation) or triggered by an external stimulus (e.g., light).

Ligands: Ions or molecules that binds to a central metal atom and which, in concert with CO, form the fundamental structure of the vast majority of CO-releasing molecules.

toxicity and rapidly reacts with hemoglobin (Hb) owing to its much higher affinity to the protein (approximately 230-fold) over molecular oxygen [8]. This event leads to the formation of carbonmonoxy hemoglobin (HbCO), inhibition of oxygen transport by red blood cells and subsequent tissue hypoxia. There is virtually no possibility of controlling tissue specificity in the administration of the gas. Consequently, CO loads tend to be high. The COVOX delivery system has now been developed by Ikaria for the administration of the gas and medical personnel will require specific training [7]. Moreover, due to safety considerations, administration of CO can at present only be carried out in hospital settings. The challenges associated with clinical application of the gas by inhalation have sparked the design of CO-RMs as an alternative approach to the administration of CO. Indeed,

CO-releasing molecules offer the possibility, through flexible chemical design, to overcome all of the problems above. Since, ideally, CO-RMs can be administered orally or via injection, the right dose of administered CO can be conveniently calculated from the known structure of the compounds. This reduces drug (and CO) loads for the patients. Tissue specificity can be controlled by chemical variation of the drugs by, for example, appending CO-RMs to receptor targeting biomolecules. If administered orally or via injection, no equipment is needed to deliver the drug and the operation may be carried out in an ambulatory setting, thus greatly reducing overall costs.

To date, the vast majority of CO-RMs are molecules tailored around a transition metal ion (FIGURE 2). In general the central metal ion is not considered to play a role in the therapeutic action of CO-RMs and it may be viewed as the scaffold for the delivery of CO. However, potentially toxic elements such as chromium, whose metabolites after CO release, would make molecules unsuitable for further advancement to become a drug should be avoided. Factors regarding the toxicity of the central metal ion are taken in great consideration, and the field has lately seen a shift in the synthesis of CO-RMs modified with biocompatible elements such as iron. CO-RMs based on purely organic molecules are also known. The only examples are the boranocarbonate species introduced by Alberto [9–11]. These molecules, along with metal-based CO-RMs, have advanced to pre-clinical trials showing promising effects as, for example, cerebroprotective agents for the treatment of epileptic seizures [12]. In this perspective article, knowledge associated with the biochemical action of CO is evaluated and the efficacy of the diatomic molecule as a therapeutic agent is discussed. Recent advances in the CO-RMs field are critically addressed and a conceptual model for the future development of the molecules is offered. The fundamental electronic and molecular orbital theory descriptions of CO-RMs are not addressed here. The reader may refer to a recent review for an in-depth discussion of these topics [13]. In this article a strong and perhaps provocative case is argued in favor of the development of targeting CO-RMs. This opinion should not be considered exclusive and certainly other approaches are valid as well. Indeed, the reader should bear in mind that in other fields of medicinal inorganic chemistry, major metal-based drugs, for example, platinum

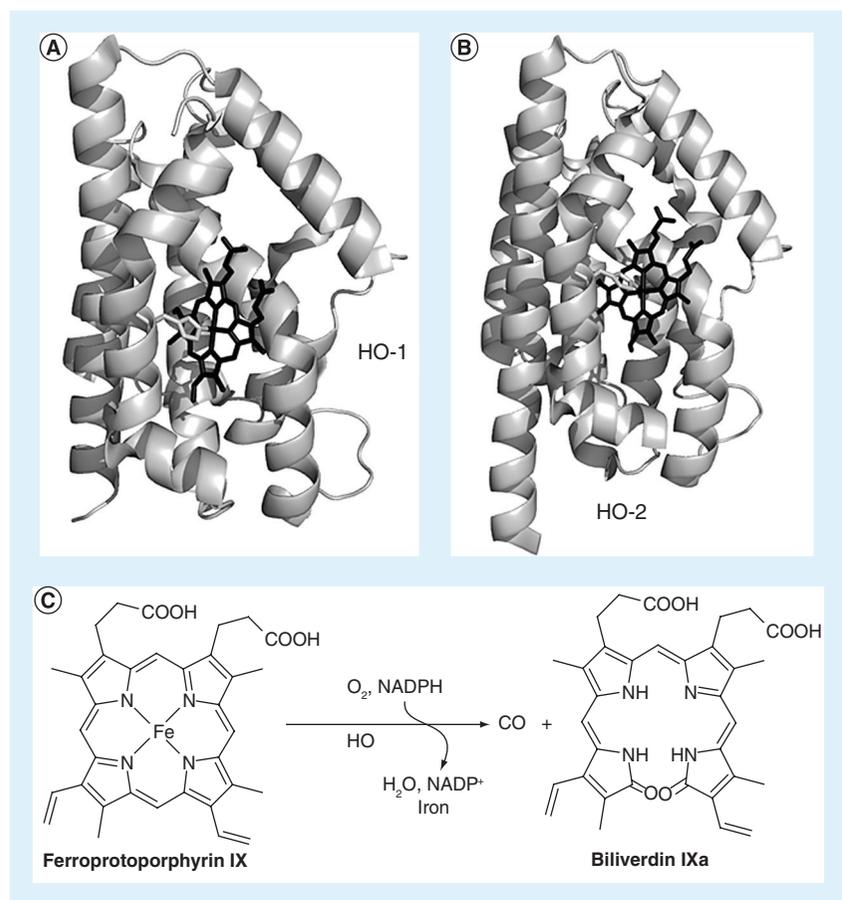


Figure 1. x-ray structures of human heme oxygenases 1 and 2 and their catalyzed heme degradation. (A) Structure of human HO-1 (PDB access code 1N45) and (B) human HO-2 (PDB access code 2QPP) in complex with their ferroprotoporphyrin IX substrate (shown in black). (C) Endogenous regioselective HO-catalyzed degradation of heme resulting into ferric iron, biliverdin IXa and a molecule of CO. HO: Heme oxygenase.

and ruthenium anticancer agents, do not possess targeting **ligands** but are very successful pharmaceuticals.

CO in biochemistry & medicine

The therapeutic effects of CO-RMs and of CO have been demonstrated in a large number of preclinical disease models. Motterlini and Otterbein have recently reviewed the medical applications of the molecules [7]. **TABLES 1 & 2** offer a brief extract of the preclinical efficacy of CO and selected CO-RMs on different disease models. A similar register may be found in the review article by Mann [1]. It should be mentioned that selected CO-RMs show similar effectiveness in the models listed in **TABLE 1** and in some cases offer a superior therapeutic action over CO inhalation alone. For instance, the bactericidal effects of a ruthenium-based CO-RM (CO-RM-3 in **FIGURE 2**) have been shown to improve survival in immunocompetent and immunosuppressed mice, while CO gas does not seem to have a direct effect on bacteria survival [14]. The way by which CO-RMs and specifically CO realize their therapeutic action is largely unknown. Indeed the biochemistry of CO is probably best understood by its toxicity [8]. Inhaled CO will cause HbCO levels to rapidly increase in the blood with consequent impairment of oxygen carrying ability and hypoxia. This event is mistakenly held responsible for the toxicity of the gas, a conviction deeply rooted in the general public and the scientific community at large. In agreement with this model, serum HbCO levels are used diagnostically in hospitals to establish the severity of CO intoxication. However, the toxicity of CO is not a simple function of serum HbCO levels and such a relationship may be applied only in cases where CO is delivered to patients in its gaseous form [13].

The issue of whether HbCO is a reliable marker of CO poisoning is of particular importance for the medical applications of CO-RMs. The answer to the problem above has actually been available in the literature for over 30 years but it was only recently brought back into sight by Foresti and Motterlini [15]. In a recent contribution, these authors have published an old comment written by Poulton in response to the work of Aronow who affirmed that blood with elevated HbCO levels should not be given to patients suffering from cardiac or pulmonary dysfunctions. Via this commentary, the 1975 work of Goldbaum on the mechanism of CO toxicity was discussed. By using groups of dogs

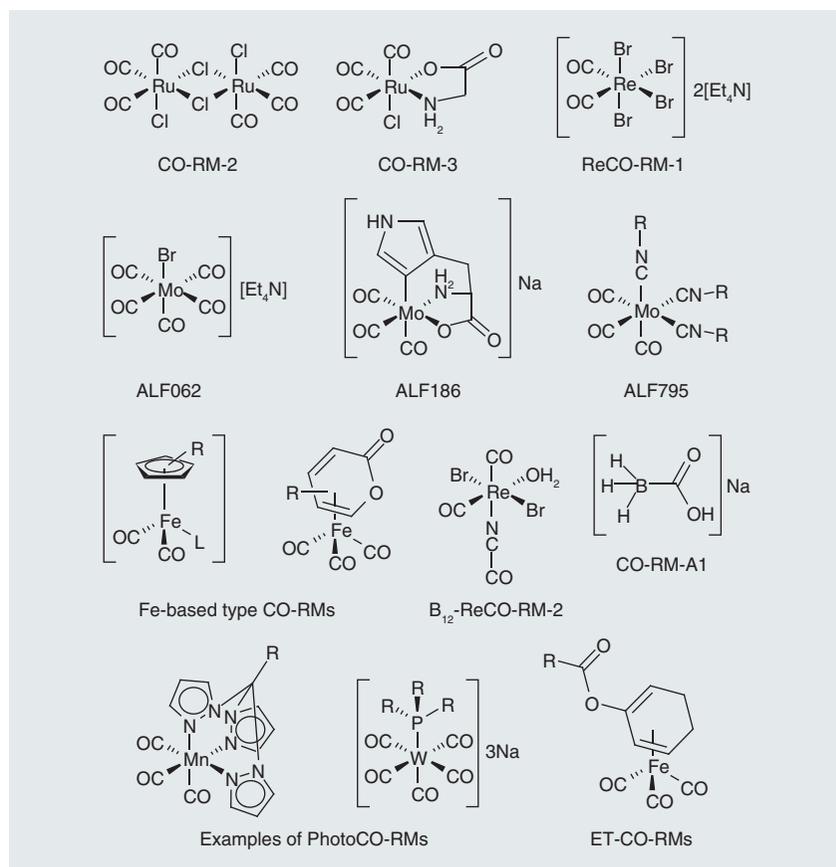


Figure 2. Structures of selected well-known CO-releasing molecules. In these examples 'R' indicates an organic substituent and 'L' a monodentate ligand. For details and references see **TABLE 2**. CO-RM: CO-releasing molecule.

that were either allowed to breathe CO or that were bled to a severe state of anemia and then transfused with red blood cells saturated with 80% HbCO, Goldbaum showed that it is not the CO bound to hemoglobin that is toxic [16]. Hb operates in a detoxifying mechanism and it is rather the fraction of CO that escapes it that becomes detrimental.

Relevant to the medicinal application of CO-RMs, the question of what is responsible for the toxicity of CO remains unanswered. But, more significantly, the therapeutic sites of action of CO are still unknown. At present, reports on the biological targets and the sites of action of CO are very limited. Cytochromes and other intracellular **hemoproteins** are often indicated as the most likely candidates [1–3,5,7,15,17]. Direct evidence of the interaction of CO with cytochromes is available [18] but several other proteins containing various transition metals, such as manganese, copper, cobalt, nickel, vanadium or molybdenum, may potentially be targeted by CO [19]. Little is known about the functional significance of such

Key Term

Hemoproteins: Believed to be the major intracellular targets of CO, they are conjugated proteins containing a metal-porphyrin compound as the prosthetic group.

Key Term**Oxidative conditioning:**

The ability of nondetrimental doses of carbon monoxide-induced reactive oxygen species generation to make cells more resistant to a subsequent insult, thus resulting in adaptation.

Table 1. Effects of inhaled CO in preclinical disease models.

Disease model	Effect of CO gas
Acute inflammation and lung injury in mice	Prevents hyperoxia-induced lung inflammation and injury
Acute liver failure in mice	Prevents liver failure and injury
Aortic allograft rejection in mice and rats	Prevents transplant vascular stenosis
Asthma and airway hyperresponsiveness in mice	Prevents bronchoconstriction and airway inflammation
Autoimmune disease in mice	Reverses paralysis
Bacterial infection in mice	Improves survival and prevents multiple-organ failure
Cardiac graft rejection in mice and rats	Prolongs survival and prevents rejection
Cardiopulmonary bypass in pigs	Reduces lung inflammation
Cerebral malaria in mice	Prevents cerebral injury
Chronic colitis in mice	Prevents colitis and inflammation
Hemorrhagic shock in mice	Prevents organ failure and improves tissue availability
Islet cell transplantation	Improves islet cell survival
Kidney and liver preservation in rats	Improves renal and liver function after treatment
Lung allograft rejection and ischemia-reperfusion injury in mice and rats	Prevents chronic rejection, ischemia-reperfusion injury and apoptosis
Myocardial infarction in mice	Prevents infarct mass
Postoperative ileus in mice, rats and pigs	Prevents ileus and improves motility
Pulmonary and renal fibrosis in mice	Prevents lung and renal fibrosis
Pulmonary hypertension in rats and mice	Reverses pulmonary artery pressure and prevents pulmonary hypertension on prolonged treatment
Sepsis and endotoxemia in mice, rats and pigs	Has anti-inflammatory effects, ameliorates lung derangement, improves survival and lung and liver injury
Sickle cell disease in mice	Prevents leukocyte infiltration and vaso-occlusion
Small bowel transplant	Prevents rejection and transplant-induced paralytic ileus

Data taken from [7] and references therein.

interactions. The physical targets responsible for mediating the protective effects of CO appear to be diverse. Often the effects of CO are found to parallel those of NO and in some cases CO action is dependent on nitric oxide production. Guanylyl cyclase is one of the rare enzymes for which direct evidence of CO modulation is available [20]. The polypeptide is activated by both CO and NO to convert guanylyl triphosphate to cGMP that then acts as an important signaling molecule. Other reports have shown that CO promotes its effects on mitogen-activated protein kinases, proliferator-activated receptors, signal transducers and activators of transcription, and hypoxia-inducible factors [21,22]. Recently, Na⁺ and calcium dependent potassium channels (K_{Ca}⁺) have been identified as potential targets of CO, owing to the HO-2 function as an oxygen sensor in these systems [23,24]. It is interesting to note here that Guanylyl cyclase is also involved in the signaling cascade that is activated by low Ca²⁺ levels and inhibited by high intracellular Ca²⁺ concentration [25].

It is now established that among the earliest cellular responses to low concentration of

exogenously applied CO is an increase in reactive oxygen species (ROS) formation. This event, called ‘**oxidative conditioning**’ [5], is particularly pertinent to the application of CO-RMs in the treatment of cardiac dysfunctions. There are several studies that support the idea that small amounts of applied gaseous CO will first affect cellular respiration resulting in local high concentration of ROS [26–29]. The downstream targets of ROS are unclear, but in response to ROS formation, cells reply with enhanced induction of antioxidant enzymes. The up-regulation of ‘conditioning enzymes’ eventually results in cellular adaptation. CO is then ascribed a (pre)conditioning role by stimulating mitochondrial ROS production and activating mitochondrial biogenesis [30–32]. Recent evidence also indicates that CO-RM-3 derived CO is capable of modulating activity of the most abundant and potent antioxidant enzymes, SOD1 and SOD2, found in all cells and tissues [27]. This mechanism, however, may not always be relevant when different CO-RMs are used for treatment instead of the gas. The promising class of rhenium-based CO-RMs

Table 2. Chemical properties and major biological effects of selected CO-releasing molecules.

CO-RM	Chemical properties	Major biological effects	Ref.
ALF062	Soluble in DMSO; unstable under aerobic conditions; $t_{1/2}$ of CO release <30 min	Effective in treatment of rheumatoid arthritis (adjuvant-induced arthritis rat model) and protects against lipopolysaccharide lethality in mice	[39,40]
ALF186	Water soluble; unstable under aerobic conditions; $t_{1/2}$ of CO release <30 min	Prevents nonsteroidal anti-inflammatory drug-induced gastric ulcer	[40]
ALF492	Water soluble; delivers approximately 1 equivalent of CO to Mb after 15 min	In combination with artesunate, fully protects mice from severe malaria	[41]
ALF795	Water soluble; stable under aerobic conditions; complete release of all CO ligands occurs within 30–45 min	Effective in treatment of acetaminophen-induced acute liver failure in mice	[42]
CO-RM-1 [$Mn_2(CO)_{10}$]	Soluble in DMSO; stable under aerobic conditions; photo-induced CO release	Dilates isolated pressurized cerebral arterioles of newborn pigs and piglet pial arterioles; attenuates inflammatory response in lungs of thermally injured mice	[43,44]
CO-RM-2	Soluble in DMSO; stable under aerobic conditions; $t_{1/2}$ of CO release at approximately 1 min	Induces vasorelaxation; attenuates inflammatory response in lungs and liver of injured mice; activates calcium dependent potassium channels (K_{Ca}^{+}); protects against ischemia/reperfusion injuries; is a possible therapeutic drug for pulmonary hypertension	[1, 44–46]
CO-RM-3	Water soluble; stable under aerobic conditions; $t_{1/2}$ of CO release at approximately 1 min	Prevents cardiac graft rejection in mice and rats; in preservation solutions improves liver and kidney function after transplant; has anti-inflammatory effects; induces vasorelaxation; prevents sepsis; effective against bacterial infection in mice; effective in treatment of rheumatoid arthritis; improves renal function; well tolerated in pigs and cynomolgus monkeys	[1,7, 14,31, 47–51]
CO-RM-A1	Water soluble; stable under aerobic conditions; rapid CO release in acidic conditions	Induces vasorelaxation; increases renal blood flow and decreases vascular resistance in mice kidneys; shows promising effects as a cerebroprotective agent for the treatment epileptic seizures	[12, 49,52]
CO-RM-F3/F6/F7/F8 [$(\eta^4-2\text{-pyrone})Fe(CO)_3$] complexes	Soluble in DMSO; stable under aerobic conditions; depending on $\eta^4-2\text{-pyrone}$ substituents, release at approximately 1 equivalent of CO within 1 h	Cause vasodilatation of precontracted aortic rings; inhibition of nitrite production in murine RAW264.7 macrophages	[53,54]
CO-RM-F10 [$CpMo(CO)_3(\text{pyrone})$] ⁺ (pyrone = 3-bromo-4-methoxy-6-methyl-2-pyrone)	Soluble in organic solvents; stable under aerobic conditions; releases 1 equivalent of CO within 1 h	Vasodilatation; inhibits nitrite production in murine RAW264.7 macrophages	[54]
[(acyloxybutadiene)Fe(CO) ₃] complexes (Enzymatically-triggered-CORMs)	Soluble in DMSO; stable under aerobic conditions; depending on acyloxybutadiene substituents, release of 0.5 equivalents of CO varies from 5 min to 8 h.	Anti-inflammatory effects based on inhibition of inducible NO synthase	[55,56]
[$Mn(CO)_5X$] (where X = Cl, Br, I)	Soluble in organic solvents; stable under aerobic conditions; $t_{1/2}$ values of CO release ranging from approximately 2 to 24 h	Bactericide activity, strongly reducing viability of <i>Escherichia coli</i> and <i>Staphylococcus aureus</i>	[101]
[$Mn(CO)_4\{\eta^2-S_2P(OEt)_2\}$]	Water soluble; stable under aerobic conditions; $t_{1/2}$ of CO release at approximately 6 min	No toxicity at 100 μ M; inhibits nitrite production in murine RAW264.7 macrophages	[102]
[$Mn(CO)_3(\text{tmp})$]PF ₆ (tmp = tris(pyrazoly)methane)	Soluble in DMSO; stable under aerobic conditions; photo-induced CO release	Photo-induced cytotoxicity against HT29 colon cancer cells comparable to the established agent 5-fluorouracil	[57]
ReCO-RM-1	Water soluble; stable under aerobic conditions; $t_{1/2}$ of CO release at approximately 6 min	Has antioxidative properties; protects neonatal rat cardiomyocyte against ischemia/reperfusion injury	[36]
B ₁₂ -ReCO-RM-2	Water soluble; stable under aerobic conditions; $t_{1/2}$ of CO release at approximately 30 min	Has antioxidative properties; protects neonatal rat cardiomyocyte against ischemia/reperfusion injury and prevents cell mortality by up to 80%	[34]

CO-RM: CO-releasing molecule.

Key Term**Photo-CO-releasing molecule:**

Any compound capable of liberating CO upon exposure to light.

(ReCORM-1 and B₁₂-ReCORM-2 in **FIGURE 2**) [33–36], for example, is able to prevent cardiomyocyte death in an ischemia-reperfusion stress model, but mitochondrial respiration is found unaffected by treatment [34]. This observation underlines the distinct possibility that different mechanisms of protection are at play in CO-RMs-based treatments when compared with gaseous CO [37]. In this specific example, the ability of the rhenium compounds to act as antioxidants might explain the lack of ROS production.

State of the art CO-RMs

The discovery, identification and design of novel CO-RMs belongs to the general discipline dubbed ‘medicinal inorganic chemistry’. The field is strongly interdisciplinary, encompassing traditional inorganic, organic and (bio) physical chemistry together with biology and medicine. The synthesis of CO-RMs, however, is currently a prerogative of inorganic chemists who are inevitably biased by their training. Consequently, at least in the early developments of the field, the literature has witnessed an explosion of molecules which, in the words of Whitty, “would be considered by a pharmaceutical company researcher to have little or no value” and “whose main claim to fame is that they show activity in a biochemical or cellular assay” [38]. The scientific value of the early synthetic studies should not be underestimated.

The vast majority of CO-RMs identified to date are molecules comprising elements of the metal transition series. Examples of selected metal-based CO-RMs that have been tested *in vitro* and/or in preclinical animal disease models are shown in **FIGURE 2** and listed in **TABLE 2** [1,7,12,14,31,34,36,39–57,101,102]. The examples provided are far from comprehensive. There are hundreds of papers describing the chemistry, the biological effects or the medical applications of CO-releasing molecules. Technically, it is not trivial to realize a metal carbonyl complex that meets all properties required for a CO-releasing agent intended as a medical drug. Beyond properties of absorption, distribution, metabolism, excretion or toxicity, inorganic medicinal chemists are faced with problems that include:

- Water solubility;
- Biocompatibility;
- Aerobic stability or stability in aqueous aerobic media;

- Rapid decay of the M(CO)_x fragment in the blood;
- Fast reactions of the metal scaffold after CO release;
- Analysis of the resulting metabolites.

To further complicate matters, inorganic chemists cannot rely on organic molecules as conceptual templates for their CO-RM design. Apart from boranocarbonate species [9–11], compounds of main group elements capable of releasing CO are rare. Some aldehydes have been used to release CO and to treat arthritis [1], but other typical examples include formic acid in concentrated sulphuric acid, dichloromethane, dimethyl formamide or other similar compounds that are beyond any possible medical applicability. Also, considering also the general mistrust surrounding the use of transition metal-based drugs in medicine, chemists involved in this field are challenged with a seemingly daunting task.

Nevertheless, several CO-RMs have been tested in preclinical disease models with remarkable success. **FIGURE 3** shows the general structure of a metal-based CO-RM. For our discussion the structure of CO-RM-3 (**FIGURE 2**) is taken as an example. The compound, of formula [Ru(CO)₃Cl(glycinate)], is undoubtedly the best known and most widely investigated CO-RM to date. Approximately 150 research articles have been published on this species. A single ruthenium atom (oxidation state 2+, d⁶ low spin system) is at the core of the molecule. Three CO ligands are arranged facially around the metal ion. A deprotonated glycine, which occupies two of the remaining coordination sites, and a single chloride ion complete the coordination sphere of the molecule. Virtually almost all known CO-RMs show this type of octahedral geometry. Variations are given by the nature and the electronic structure of the central metal ion, the number and the spatial arrangement of the CO groups, and the type, number and coordination mode of the ancillary ligands [58,59]. Beyond structural considerations, for the purpose of this article, state-of-the-art metal-based CO-RMs will be broadly divided in two classes. The first class of molecules comprises CO-RMs in which CO release is either spontaneous or initiated by hydrolysis or redox reactions at the metal core [33–36,42,54,60–66]. The second class encompasses molecules for which external stimuli (e.g., light) are required in order to promote CO dissociation [55,56,57,67–76].

Mechanisms of CO release

In the simplest conceptual case, CO-RM reactions leading to CO loss may be ascribed to CO dissociation from the metal ion. Both theoretical and experimental studies have shown that CO dissociation is a facile step in several Mn- and Fe-based CO-RMs bearing dithiocarbamate ligands. In buffer solutions, an equilibrium involving release and re-coordination of CO is rapidly established in this family of compounds [64,77–79]. A second possible mechanism of CO release is generally referred to as a hydrolytic or thermal process. In this class of molecules, aquation or ligand substitution at the metal centre triggers CO release. The steps leading to CO loss are not entirely understood, but it is reasonable to assume that CO is liberated via an acid/base-catalyzed, an associative, or a dissociative substitution mechanism. The latter may also be pH dependent. Possible mechanisms leading to CO loss are outlined in **FIGURE 3**. Often, however, the detailed description of CO release is more complicated than the simple scheme portrayed in **FIGURE 3**. Redox processes at the metal centre also play a role in the liberation of CO. The recently described Fe complexes with polypyridyl ligands might exemplify this issue [75]. For these compounds it has been reported that the CO-releasing behavior is critically dependent on the presence of dioxygen. The molecules are thus stable under anaerobic conditions and their CO loss has been attributed to the formation of a highly stable μ -oxo diiron species (i.e., a molecule with a Fe–O–Fe bond).

The hydrolytic and redox processes are not mutually exclusive. A class of CO-RMs based on electronically unsaturated Re complexes (ReCO-RM-1 and B_{12} -ReCO-RM-2 in **FIGURE 2**), appears to release CO via a combined path of mechanisms (**FIGURE 4**) [34]. When dissolved in aqueous media, three bromides in ReCORM-1 are rapidly exchanged for solvent molecules. The substitution of three Br⁻ by three water molecules is postulated to increase the Re^I \rightarrow Re^{II} redox couple of **1a** (**FIGURE 4**) to a value sufficient to drive the oxidation of Br⁻ to BrO⁻. Following reduction of the solvated Re^{II} complex the corresponding Re^I species is formed (**1b**; **FIGURE 4**). This complex is then proposed as the CO-releasing entity liberating one equivalent of CO within 30 min under physiological conditions. In aqueous solutions under aerobic conditions, the monocarbonyl Re^I complex is finally oxidized to the non-toxic ReO₄⁻ anion. Complexes of electronically unsaturated

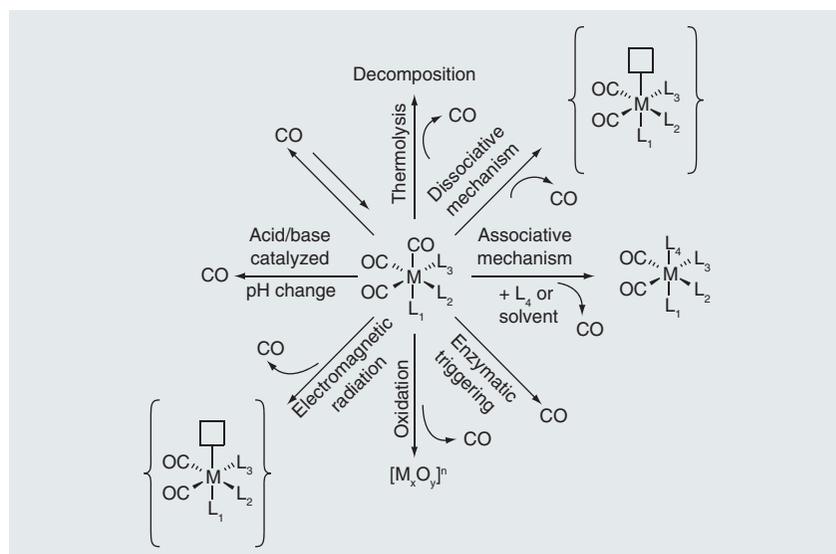


Figure 3. Possible reactions resulting in the CO loss from a CO-releasing molecule of general formula $[(CO)_3ML_1L_2L_3]$. The loss of CO may be either spontaneous (e.g., thermolysis, pH change) or triggered by an external stimulus (e.g., electromagnetic radiation or enzymatic activation).

Re-based CO-RMs are a rare example for which both a tentative mechanism of CO loss and the final metabolite have been elucidated.

Within this first set of molecules, borano-carbonate compounds of formula $Na[H_3BCO_2H]$ (CORM-A1 in **FIGURE 2**) and $Na[H_3BCONR_2]$ (where R = organic functionality) deserve to be mentioned briefly [9–11,79]. These represent the only group of nontransition-metal compounds that release CO. At physiological pH these molecules lose CO via an acid/base-catalyzed mechanism. CORM-A1 shows potential as a cerebroprotective agent for the treatment of epileptic seizures [12], it is active in the cardiovascular system [52] and reduces inflammation [80,81]. More than 30 papers have been published on biological applications of this compound.

The second broad class of CO-RMs are molecules for which external stimuli (e.g., light or enzymatic activation) are required in order to promote CO dissociation. Complexes comprising the $[Mn(CO)_3]^+$ core are the best-known examples of light-activated CO-RMs (**FIGURE 2**) [57,70–72,74]. These compounds, now called ‘photo-CO-RMs’ [69], are being developed in order to address some of the fundamental problems associated with the delivery and the tissue specificity of the drugs. Once the biodistribution of the drug is elucidated, photochemical cleavage of CO allows in principle to control the timing, dosage and the location of the released CO. At present, the limitation of photo-CO-RMs

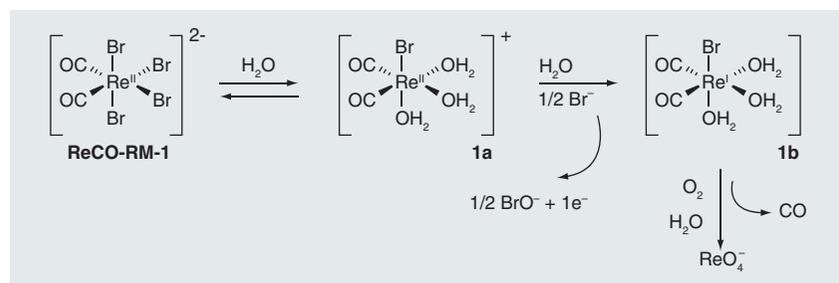


Figure 4. The proposed mechanism underlying the CO loss from an electronically unsaturated Re-based CO-releasing molecule, and its subsequent oxidation to the ReO_4^- anion.

Adapted from [34].

is in the radiation wavelength at which they are activated. Generally photo-CO-RMs are activated with high-frequency light in the UV range ($h\nu < \text{approximately } 400\text{nm}$) but examples are known of complexes where higher wavelengths can be used to promote CO loss. The $[\text{Fe}(\text{SCH}_2\text{CH}_2\text{NH}_2)_2(\text{CO})_2]$ complex, for example, can be activated with a wavelength of 470 nm [82]. Thus, in general, photochemical triggering is a technique currently limited to *in vivo* applications to sites directly exposed to the body's surface. This represents perhaps the most pressing problem for the photo-CO-RMs community. In the words of Schatzschneider: "The main challenge in the further development of photo-CO-RMs will be to prepare compounds in which the photolytic release of CO can be triggered by light in the phototherapeutic window, that is at wavelengths above 600 nm" [71]. Three solutions have been proposed to meet the challenge above: the bathochromic shift of absorption maximum of the photo-CO-RMs via ancillary ligands with extended aromatic π -systems; the use of photo-CO-RMs with appended photosensitizers to aid in the liberation of CO; the simultaneous absorption of two photons of identical or different frequencies to promote the CO releasing process via the two-photon absorption technique [71].

Enzymatically triggered CO-releasing molecules (ET-CO-RMs) are a new and interesting class of CO-RMs that have recently appeared in the literature [55,56]. The compounds, based on acyloxybutadiene tricarbonyl iron species (FIGURE 2), are activated by intracellular esterases, which, upon cleavage of the ester functionality on the acyloxybutadiene precursors, generate a highly unstable hydroxybutadiene ligand on the iron center. This reaction triggers decomposition of the molecule via oxidation of the $[\text{Fe}(\text{CO})_3]$ core ultimately leading to CO

release. This strategy represents a new concept in the development of CO-RMs [55,56]. ET-CO-RMs show strong inhibition of inducible nitric oxide synthase, but their activation is currently limited to a restricted number of enzymes. Some toxicity issues still need to be addressed in this class of CO-RMs.

Systemic or targeted drugs?

CO-RMs are unlike most drugs whose pharmacological action is dependent on their interaction with a macromolecular target and whose potency is dictated by the duration of the drug-target complex persistence. In most cases, modulation of such drug-target interactions are achieved by chemical variation on the periphery of the compound. Apparently small changes (as it might be the substitution of a methyl for an ethyl group) have profound consequences on the effectiveness of the drug due to conformational and structural changes around the pharmaceutical binding pocket of the macromolecule that in turn controls the dynamics of drug dissociation. CO-RMs, however, are believed to exert their therapeutic action via a completely different mechanism. Presently, they are not designed to target a specific receptor and their potential utility is generally ascribed to their fundamental ability to liberate CO. CO-RMs are **systemic prodrugs**; CO is their 'active ingredient'. Thus, CO-RMs must survive long enough under physiological conditions and be activated only at the disease site. The half-life of the drug (e.g., in the circulatory system) is considered of great importance for the therapeutic effectiveness of the molecule. Significant research efforts continue to be dedicated to the design of CO-RMs with suitable ligands capable of modulating the half-life of CO-loss. Very recently, Atkin pointed out that "due to the diverse nature of the applications (i.e., of CO-RMs), the optimum release rate for CO release is not known; thus, the development of a variety of CO-RMs with different activities is desirable" [83]. This is a valid argument, but other factors will play a decisive role for the advancement of CO-RMs as acceptable pharmaceuticals.

It is now established that for any given transition metal-based CO-RM, the rate of CO release is influenced by the electronic structure of the metal and by the atoms directly bound to it. This selection of ligands forms what is defined in inorganic chemistry as the first coordination sphere of the metal ion. The development of

Key Terms

Enzymatically triggered CO-releasing molecules:

Molecules capable of liberating CO as a result of an enzymatic reaction. In general considered to be recognized as a substrate of the selected enzyme.

Systemic prodrugs:

CO-releasing molecules with no targeting functionalities, which, once administered orally or intravenously, are expected to act (i.e., release CO) on the whole body.

clinically useful transition metal-based CO-RMs, however, must move beyond the simple inorganic chemistry approach. In parallel to the identification and design of, for example, octahedral, tetrahedral or square planar carbonyl complexes, the new frontier of CO-RMs research needs to address issues relevant to basic physicochemical properties required for an acceptable pharmaceutical behavior. These issues were also addressed by Romão and his team in a recent tutorial review on the development of therapeutic CO-RMs [13]. In their contribution, the authors have described a conceptual CO-RM model that takes into account both the first coordination sphere of the central metal and a second expanded sphere that they named the ‘dug sphere’ of the molecule. There it was argued that, within the constraints of metal carbonyl chemistry, modifications of the drug sphere should be considered to modulate drug-like features of CO-RMs, and in turn address absorption, distribution, metabolism and excretion properties. Targeting functionalities could also be introduced within this second sphere.

We believe this is a valid model. Indeed, amino acids, purine and pyrimidine bases have been used since the beginning in the design of CO-RMs as the presence of such molecules removes toxicity issues of released ligands. We have also prepared biocompatible site-specific metal based-CO-RMs conjugated to biomolecules. Specifically, we have introduced cyanocobalamin (vitamin B12) within the drug sphere of labile Re(II)-based CO-RMs [34]. The idea behind the development of such bio-conjugates is to target the metallo prodrug to a specific location within the organism and thus elicit a compartmentalized homeostatic response as opposed to a systemic one that is chaotic and disordered. This goal may only be achieved by functionalizing CO-RMs with receptor targeting biomolecules in order to ensure, at least theoretically, the exclusive accumulation of the drug in the diseased organ or tissues that are intended to be treated. It is this approach that is now driving our CO-RM research program. The strategy is shown in **FIGURE 5** – a bio-conjugated CO-RM designed for a specific target (and/or receptor) is anticipated to accumulate preferentially at the site of interest. CO-RM decomposition (i.e., CO release) follows the bio-carrier mediated target binding, thereby promoting CO passive diffusion and accumulation at the target location. It should be noted, however, that it is currently possible to administer CO-RMs locally for many of the potential

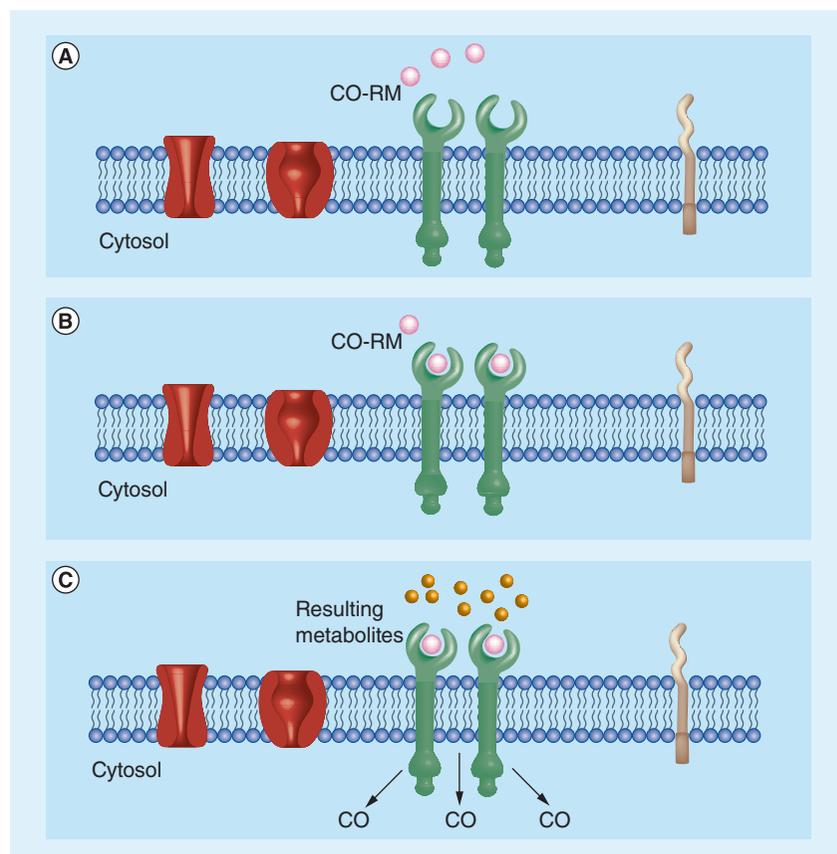


Figure 5. Development of biocompatible-site specific metal-based CO-releasing molecules. (A) Bio-conjugate CO-RM approach to target site. **(B)** Bio-carrier mediated receptor binding. **(C)** CO-RM decomposition, CO release and CO penetration at target site. CO-RM: CO-releasing molecule.

applications. It is known that ALF062, CORM-3 and $[\{HC(C_3H_3N_2)_3\}Mn(CO)_3]^+$, for example, enter cells and as a result are likely to remain close to the site of administration [18,39,84].

Nevertheless, the careful selection of targeting functionalities within the drug sphere of CO-RMs will not only allow a compartmentalized therapeutic effect, but will aid in overcoming the general poor water solubility of the metal complexes. Furthermore, the modulation of the drug sphere should bring CO-RMs to behave more like standard organic drugs *in vivo*. Thus, depending on the strength and persistence of the CO-RM-target (and/or receptor) complex, it would be possible to select CO-RMs with different CO-releasing profiles to promote either a rapid (i.e. with CO-RMs with short half-lives) or a continual therapeutic action. These effects could also be achieved with appended CO-RMs capable of releasing two or more equivalents of CO at different rates. Overall, this strategy should ultimately result in a reduced drug load for patients.

Future perspective

The field of CO-releasing molecules is certainly gaining momentum. An increasing number of scientists are entering the CO-RM arena and in the near future we are likely to face a growing number of molecules identified for this purpose. Certainly the field will still require the invaluable input of synthetic chemists, but a shift must also occur towards more application-oriented studies. Only a small fraction of the published compounds has advanced beyond the initial biological tests. A number of private companies (e.g., ALFAMA) are currently

exploring the possible commercial value of CO-RMs. Due to patenting issues, it is likely that within the next 5 to 10 years compounds of significant medicinal value will appear in literature. Their structures will provide a new synthetic platform for the advancement of the field. At present, however, there are several problems to be solved [85]. The need to address issues relevant to basic physicochemical properties required for an acceptable pharmaceutical behavior was discussed above. In addition to that, from a chemical standpoint, more efforts should be directed towards the elucidation of

Executive summary**Background**

- CO-releasing molecules (CO-RMs) and their action-derived CO mediate therapeutic effects in different pathological conditions.
- CO and CO-RMs have advanced in a wide range of medical applications. These include organ transplantation and preservation, reduction of reperfusion injury, inflammation, sepsis and killing drug-resistant bacteria.

CO in biochemistry & medicine

- CO-RMs and CO realize their therapeutic action via largely undetermined mechanisms.
- The biological targets of CO are unknown, but cytochromes and other hemoproteins are indicated as the most likely candidates.
- CO is ascribed a (pre)conditioning role by stimulating mitochondrial reactive oxygen species production and activating mitochondrial biogenesis.

State of the art CO-RMs

- The vast majority of CO-RMs are molecules tailored around a transition metal ion.
- Virtually almost all known metal-based CO-RMs show an octahedral geometry.
- CO-RM design should take into account absorption, distribution, metabolism and excretion properties, toxicity, water solubility and biocompatibility.

Mechanisms of CO release

- CO-RMs may be broadly divided in to two types of classes: molecules in which CO release is either spontaneous or initiated by hydrolysis or redox reactions at the metal core, and molecules for which external stimuli are required in order to promote CO dissociation.
- In the simplest conceptual case, CO-RM reactions leading to CO loss may be ascribed to CO dissociation from the metal ion.
- A second possible mechanism of CO release is generally referred to as a hydrolytic or thermal process.
- CO-RMs for which external stimuli are required to promote CO dissociation are known as photo-CO-RMs (for light-activated molecules) or enzymatically-triggered CO-RMs.
- Boranocarbonate compounds are the only group of non-transition-metal CO-RMs.

Systemic or targeted drugs?

- CO-RMs are currently not designed to target specific receptors or macromolecules. They can be defined as systemic prodrugs.
- The new frontier of CO-RMs research needs to consider issues relevant to basic physicochemical properties required for an acceptable pharmaceutical behavior.
- A possible solution to address absorption, distribution, metabolism and excretion properties is via the formation of CO-RM-bio-conjugate systems capable of targeting a specific location within the organism and thus elicit a compartmentalized homeostatic response as opposed to a systemic one that is chaotic and disordered.

Future perspective

- In the near future the field will likely see a shift towards more application-oriented studies.
- Due to the involvement of private companies exploring the commercial value of CO-RMs, it is likely that within the next 5 to 10 years, compounds of significant medicinal value will appear in literature.
- The main focus of medicinal chemists should also be directed towards the generation of CO-RMs that are tissue specific, so as allow a controlled delivery of CO.
- Targeted delivery is, however, one of the other valid approaches.
- Initiatives to foster more intensive collaborations among research groups are being promoted.

the mechanistic details underlying CO release. Several authors have already made important contributions and, in this respect, the work of Fairlamb, Lynam and Mann is exemplary. The identification of metabolites resulting after CO release or decomposition of CO-RMs also requires more rigorous scientific investigation. Unlike the simple gas, CO is delivered by CO-RMs on a metal scaffold. The fate of the metal backbone must be elucidated from a metabolic and toxicological point of view. Existing techniques for the measurements of the CO release need to be perfected. Currently, CO detection is achieved spectroscopically either by trapping CO with myoglobin or hemoglobin, or with gas chromatography, CO electrodes or *in situ* infra-red techniques. It would be advantageous for the community to develop a common reliable method that could be used as the standard for all. The widely spread myoglobin assay has shortcomings. This was clearly demonstrated in recent studies [86–88]. The main focus of medicinal chemists should be directed towards the generation of CO-RMs that are tissue specific, so as to allow a controlled delivery of CO. Targeted delivery is, however, one of the other valid approaches. Thus, for example, it is acknowledged that for treatment of infections such as infected wounds, the local administration of creams containing CO-RMs is advantageous

over molecules designed to target CO-RMs to tissues or organs, just as the use of aerosols is superior for the treatment of lung infections. All the issues above are openly discussed in the community and concrete steps forward have already been made. Initiatives to establish a solid network among research groups are being promoted. These include the creation of a publicly accessible CO-RM library where synthetic procedures, CO-releasing profiles, the biodistribution and the therapeutic effects of different molecules are collected. Steps are being taken to foster more intensive collaborations between chemists, biologists and medical doctors in order to fully realize the potential of CO-RMs. This is probably the only possible solution to meet the ultimate challenge in the field: bringing CO-RMs into clinical use.

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■ Patents

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