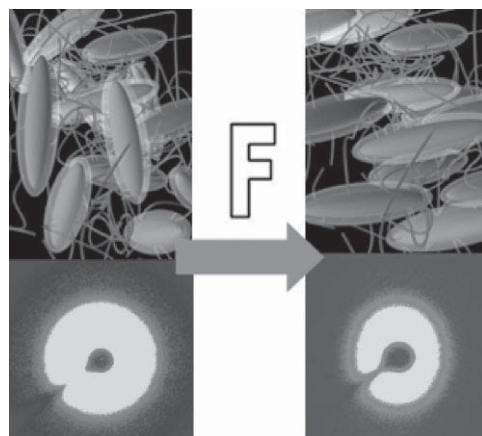


Orientational Behavior of Ellipsoidal Silica-Coated Hematite Nanoparticles Integrated within an Elastomeric Matrix and its Mechanical Reinforcement

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The mechanical and orientational properties of IOENs consisting of integrated ellipsoidal SCH spindle-type nanoparticles within an elastomeric matrix are reported. The influence of the SCH surface chemistry, leading either to dispersed nanoparticles or crosslinked nanoparticles within the surrounding elastomeric matrix, is studied by mechanical uniaxial deformation (stress-strain) and SAXS measurements under stress. Without surface modifications, the SCH nanoparticles act as defects, and the Young's modulus of the elastomeric matrix remains unmodified. Surface-modified SCH nanoparticles acting as crosslinkers increase Young's modulus by a factor 1.2. SAXS measurements demonstrate that the integrated ellipsoidal nanoparticles orient upon a deformation larger than 50% independently of the specific integration strategy.



Introduction

Hybrid nanocomposite materials made out of integrated inorganic nanoparticles within an organic polymeric matrix can be found as gels,^[1] thermoplastics,^[2] thermosets or elastomers.^[3] This class of materials can exhibit the combined advantages of both the integrated nanoparticles, in terms of optical and electrical properties, and the processability of the polymeric matrix. As a result, bulk modification of the strength, stiffness, and toughness of the resulting materials are generally observed.^[4,5]

Different approaches have been reported in the past for the integration of nanoparticles within a polymer network leading to nanocomposites, including particle/polymer hydrogels,^[6] particle/elastomer composites,^[7–10] silica-thermoset networks via in situ polymerization,^[11] or linear polymer networks induced by particles.^[12] In most cases, aggregation and migration of the integrated fillers under an external trigger (e.g., electrical field, magnetic field, or a high shear rate) appears as a drawback of this specific route.

A potential solution is to integrate the nanoparticles in a covalent manner, binding them to the polymer backbone, which leads to a cooperative motion of both the continuous and dispersed phases.^[3,11,13–14] In this way, potential phase separation of the integrated nanoparticles can be avoided or reduced. Few examples can be found in the literature of integrating anisometric nanoparticles within a polymer matrix, and most of those are polymer/clay nanocomposites^[15–17] or block copolymer/carbon nanotube nanocomposites,^[18,19] with improvement of mechanical properties,

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but still with aggregation of the nanoparticles in clusters. Two recent successful works on the integration of wires into a liquid-crystalline polymer network,^[20] and ellipsoidal nanoparticles into block copolymers^[21] were also reported. So far, no examples are available where anisometric nanoparticles are present in a chemical elastomeric network as crosslinkers, and the mechanical and orientational behavior of both nanoparticles and polymer matrix are studied in detail. In this context, a strategy towards inorganic/organic elastomer nanocomposites (IOENs) was also recently proposed using silica-coated hematite (SCH) which was integrated within an elastomeric matrix.^[22] Evidence concerning the quality of the dispersion and distribution of the nanofillers within the matrix was obtained for surface-treated SCH with one of both functionalities taking part in the polyaddition process.^[3] However, the impact on the structural and mechanical properties provided by the presence of integrated nanoparticles within the elastomeric matrix was not disclosed, which is the main motivation for the present work.

In the current study we investigate whether integrated ellipsoidal nanoparticles can both mechanically reinforce an elastomeric matrix and orient under stress (i.e., coupling between the polymer network and the nanoparticles). To this end, nanoparticles acting as crosslinkers or mixed in an uncontrolled way have been compared at an equivalent filler concentration and evaluated by both classical mechanical tests and scattering patterns under mechanical stress.

Experimental Part

Materials

Iron(III) perchlorate hexahydrate [$\text{Fe}(\text{ClO}_4)_3 \cdot 6\text{H}_2\text{O}$], poly(vinylpyrrolidone) (PVP, $10\,000\text{ g} \cdot \text{mol}^{-1}$), and a 25% solution of tetramethylammonium hydroxide (TMAH) in methanol were all provided by Sigma-Aldrich and used as received. Sodium dihydrogen phosphate monohydrate ($\text{NaH}_2\text{PO}_4 \cdot \text{H}_2\text{O}$), urea, and absolute ethanol were provided by Fluka. Tetraethylorthosilicate (TEOS) and acetone were provided by Merck, and 3-aminopropyltriethoxysilane (APTES) from ABCR, were also used without further purification. Ultrapure water ($18.2\text{ M}\Omega \cdot \text{cm}$) purified by a MilliQ system, was used throughout the experiments. The diamine-terminated poly(propylene oxide) polymer Jeffamine D-2000 with approximate number-average molecular mass (\bar{M}_n) of $2\,000\text{ g} \cdot \text{mol}^{-1}$ was kindly provided by Huntsman Corporation and degassed before use. The triisocyanate crosslinker Basonat HI-100 was kindly provided by BASF SE and used as received.

Synthesis of Ellipsoidal SCH Nanoparticles

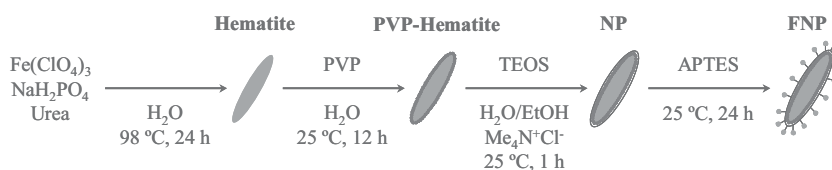
An aqueous solution of iron(III) perchlorate (0.100 M), sodium phosphate monobasic ($5.5 \times 10^{-3}\text{ M}$), and urea (0.100 M) was kept in

an oven at 98°C for 24 h. The precipitated nanoparticles were then washed five times by centrifugation at $10\,000\text{ rpm}$ for 15 min followed by redispersion in water using an ultrasonic bath. Nanoparticles (150 mg) were dispersed in a solution of PVP (surface density of $13\text{ PVP molecules} \cdot \text{nm}^{-2}$). The suspension was stirred for 12 h to let the polymer adsorb onto the surface. The stabilized nanoparticles were then transferred in 485 mL of a $17.497:82.488:0.015\text{ v/v}$ mixture of water/ethanol/tetramethylammonium chloride (25% solution in methanol). While stirring and sonicating, a 1:2 mixture of TEOS and ethanol was added in three portions of 6 mL each every 20 min.^[23,24] For surface-functionalized nanoparticles, 30 min after the last TEOS addition, $160\text{ }\mu\text{L}$ of APTES was added. Sonication was applied for 2 h after the last injection and the mechanical stirring was further continued overnight at room temperature. The nanoparticles were then washed by centrifugation and redispersion. After adding acetone to the aqueous nanoparticle dispersion, the precipitate was washed five times by centrifugation at $10\,000\text{ rpm}$ for 15 min, followed by redispersion in acetone using an ultrasonic bath. The final concentrations of functionalized SCH nanoparticles and normal SCH nanoparticles were 1.4 and $2.8\text{ mg} \cdot \text{mL}^{-1}$, respectively. The synthetic route to obtain the ellipsoidal SCH nanoparticles, i.e., the crosslinkable functionalized nanoparticles (FNPs) and non-crosslinkable nanoparticles (NPs), is shown in Scheme 1.

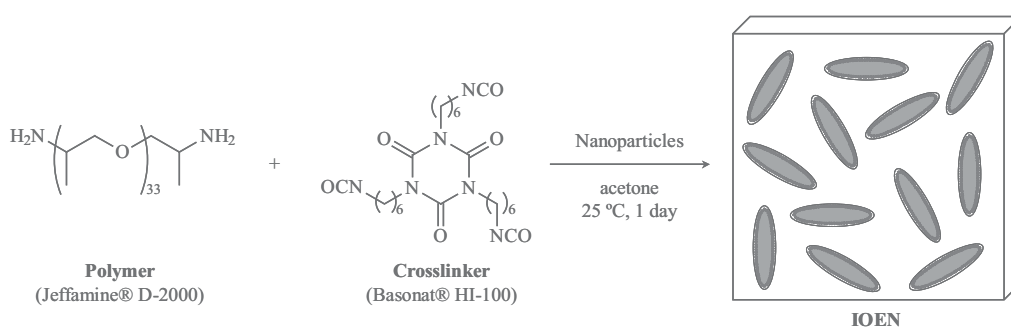
From scattering and transmission electron microscopy (TEM) experiments,^[3,25] the prolate spheroid nanoparticle ($a > b = c$) radii were calculated, and for the FNPs, values of $a = 129\text{ nm}$ and $b = 26\text{ nm}$ were found. The NPs had radii of $a = 114\text{ nm}$ and $b = 23\text{ nm}$. Both types of nanoparticles had a shell thickness of $s = 4.8\text{ nm}$. The polydispersity of the hematite core was 0.5, while that for the silica shell was 0.2.

Synthesis of IOENs

Three elastomers were synthesized: a reference elastomer (E0) without any nanoparticle, and two elastomers containing SCH nanoparticles (E1 and E2). The two SCH nanoparticles in the matrix were either functionalized with amino groups on the surface of the silica-coated hematite (FNP for E1), or bare silica coated hematite nanoparticles (NP for E2). For the synthesis of the three elastomers, two solutions in acetone were prepared: one containing the diamino-terminated polymer, and the other the trifunctionalized crosslinker with or without nanoparticles. In order to obtain a final solid content of 15 w/v , 3.85 g of Jeffamine D-2000 was dissolved in 11.1 mL of acetone, and 0.65 g of Basonat HI-100 was dissolved in 14.5 mL of acetone. In the case of elastomers containing SCH nanoparticles, the Basonat HI-100 was dissolved in an acetone dispersion of the corresponding nanoparticles to be incorporated. The two solutions were mixed and gently stirred for 5 min, and



Scheme 1. Synthetic route to obtain the ellipsoidal SCH nanoparticles (NP: non-crosslinkable nanoparticles; FNP: crosslinkable functionalized nanoparticles).



■ **Scheme 2.** Chemical structures of the organic components for the synthesis of IOENs.

the final solution was cast onto the glass surface of a Petri dish. One day after the samples were cast, the obtained film was allowed to dry in the atmosphere and peeled from the surface.^[3,22] Samples were cut from their corresponding free-standing films ($14.6 \times 5.0 \times 0.75 \text{ mm}^3$).

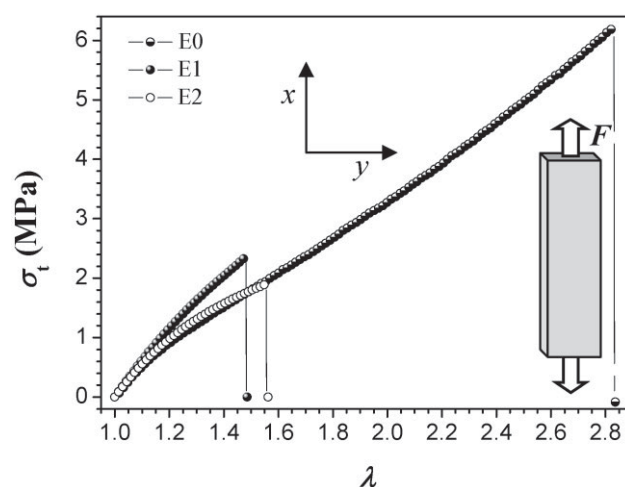
The theoretical concentrations of nanoparticles in the two samples were $c(\text{E1}) = 0.48 \text{ wt.}\%$ and $c(\text{E2}) = 0.88 \text{ wt.}\%$, which correspond to 0.11 and $0.20 \text{ vol.}\%$, respectively. These concentrations correspond to 2.1×10^{12} and $5.5 \times 10^{12} \text{ particles} \cdot \text{cm}^{-3}$, respectively. For a homogeneous distribution of nanoparticles, these concentrations lead to a distance between two neighboring nanoparticles in the elastomeric matrix of about $500\text{--}700$ and $300\text{--}500 \text{ nm}$, respectively (the lower limit corresponds to the long axis distance and the upper limit to the short axis distance). The materials and preparation of the inorganic nanoparticles, as well as their integration into the polymer network, is depicted in Scheme 2. Figure 1 presents the films and their optical and TEM pictures, where sample E1 shows a good dispersion of the FNPs.

Apparatus and Techniques

Uniaxial stress-strain measurements were performed with a Linkam TST350 thermostatted tensile testing system and controlled by a T95-LinkSys controller. Samples were stretched by two

controlled microstep motors at an extension rate of $10 \mu\text{m} \cdot \text{min}^{-1}$, which corresponded to a strain rate of $1.14 \times 10^{-5} \text{ s}^{-1}$. The stress was measured by a transducer load cell (tensile force of 20 N ; force resolution 0.001 N). All relevant data such as temperature, uniaxial strain ratio ($\lambda = L/L_0$, where L and L_0 are the lengths of the film in the stretched and nonstretched states), and nominal uniaxial stress (σ_n) were continuously logged by Linksys 32 AV software.

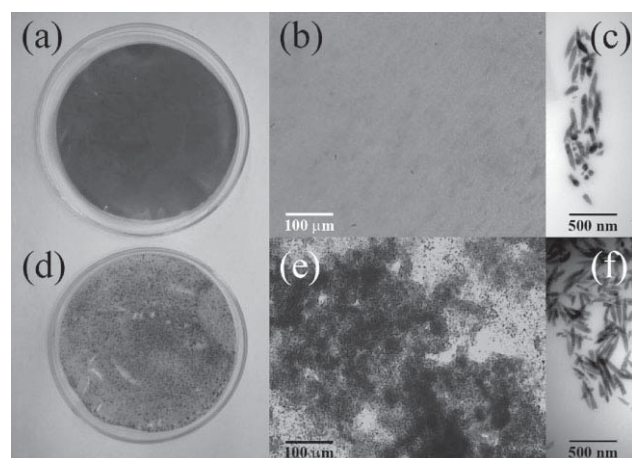
Simultaneous small and wide-angle X-ray scattering (SAXS and WAXS, respectively) experiments were performed using a Rigaku MicroMax-002+ microfocused beam (4 kW , 45 kV , 0.88 mA) in order to obtain direct information on the SAXS and WAXS reflections. The



■ **Figure 2.** Uniaxial stress-strain curves for the three elastomeric nanocomposites E0, E1, and E2, and definition of the direction of deformation. Note: $\sigma_t = \lambda \cdot \sigma_n$

■ **Table 1.** Young's modulus (E), maximum strain (λ_{max}), energy at $\lambda = 1.48$ (U), and toughness (U_{max}) for the three elastomeric samples.

Sample	E MPa	λ_{max}	$U (\lambda = 1.48)$ $\text{J} \cdot \text{cm}^{-3}$	U_{max} $\text{J} \cdot \text{cm}^{-3}$
E0	5.1 ± 0.1	2.83	0.47	5.68
E1	6.2 ± 0.1	1.48	0.62	0.62
E2	5.3 ± 0.1	1.56	0.50	0.64



■ **Figure 1.** a) Sample E1 and its corresponding optical microscopy image (b) and TEM image (c). d) Sample E2 and its corresponding optical microscopy image (e) and TEM image (f).

Cu K_{α} radiation ($\lambda_{\text{Cu } K_{\alpha}} = 1.5418 \text{ \AA}$) was collimated by three pinhole (0.4, 0.3, and 0.8 mm) collimators. The incident beam was normal to the surface of the film. The scattered X-ray intensity was detected by a Fuji Film BAS-MS 2025 imaging plate system ($15.2 \times 15.2 \text{ cm}^2$, $50 \mu\text{m}$ resolution) and a two-dimensional Triton-200 X-ray detector (20 cm diameter, $200 \mu\text{m}$ resolution). An effective scattering-vector range of $0.05 \text{ nm}^{-1} < q < 25 \text{ nm}^{-1}$ was obtained, where q is the scattering wave-vector defined as $q = 4\pi \sin \theta / \lambda_{\text{Cu } K_{\alpha}}$, with a scattering angle of 2θ . From the scattering intensities, the order parameter (S) was defined according to Lovell and Mitchell.^[26,27]

A Leica DM LB optical microscope equipped with a Linkam CSS450 hot-stage was used to analyze the homogeneity of the samples.

TEM images were obtained with a Philips TEM (CM 100) instrument operated at 80 kV. The elastomeric samples were cryo-ultramicrotomed at -80°C using a diamond knife on a Leica Ultracut UCT Ultramicrotome to give 50 nm thick sections. Sections were then transferred onto 600-mesh carbon-coated copper grids.

Results and Discussion

Uniaxial Deformations

Mechanical deformations are a very suitable way to understand the effect of nanoparticles as reinforcement in polymeric matrices. Furthermore, the combination of uniaxial stress-strain experiments together with X-ray measurements is a powerful technique to understand both the structural and mechanical processes taking place during deformation.

The resulting curves are presented in Figure 2, where the reference sample (E0) shows a common elastomeric behavior. In the elastic region, during the first deformation steps, the Young's modulus can be calculated following the relation $E = d\sigma/d\lambda$. In this way, the two samples containing nanoparticles (E1 and E2) and the reference sample were uniaxially deformed, and the restoring force measured at each stretching step. The evaluation of the initial slopes for each sample shows a difference when FNPs or NPs are present in the hybrid nanocomposite. The elastomer containing FNPs (E1) has a Young's modulus of $E_1 = 6.2 \pm 0.1 \text{ MPa}$,

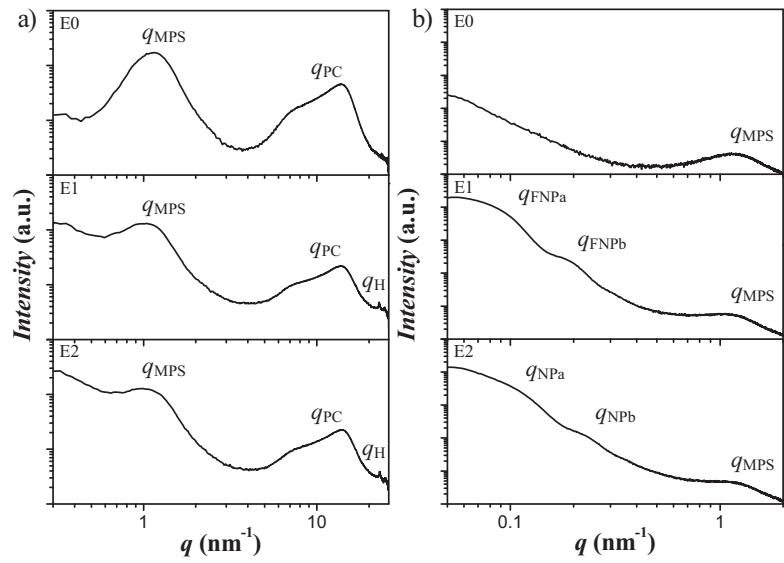


Figure 3. a) WAXS and b) SAXS radial scattering distributions for the three elastomeric samples E0, E1, and E2.

whereas the elastomer with NPs (E2) has a Young's modulus $E_2 = 5.3 \pm 0.1 \text{ MPa}$, similar to the corresponding value for the reference elastomer (E0) of $E_0 = 5.1 \pm 0.1 \text{ MPa}$. This difference of 20% in the Young's modulus for the elastomer E1 with respect to the elastomer E2 shows how the nanoparticles as crosslinkers enhance the mechanical properties of the nanocomposite.

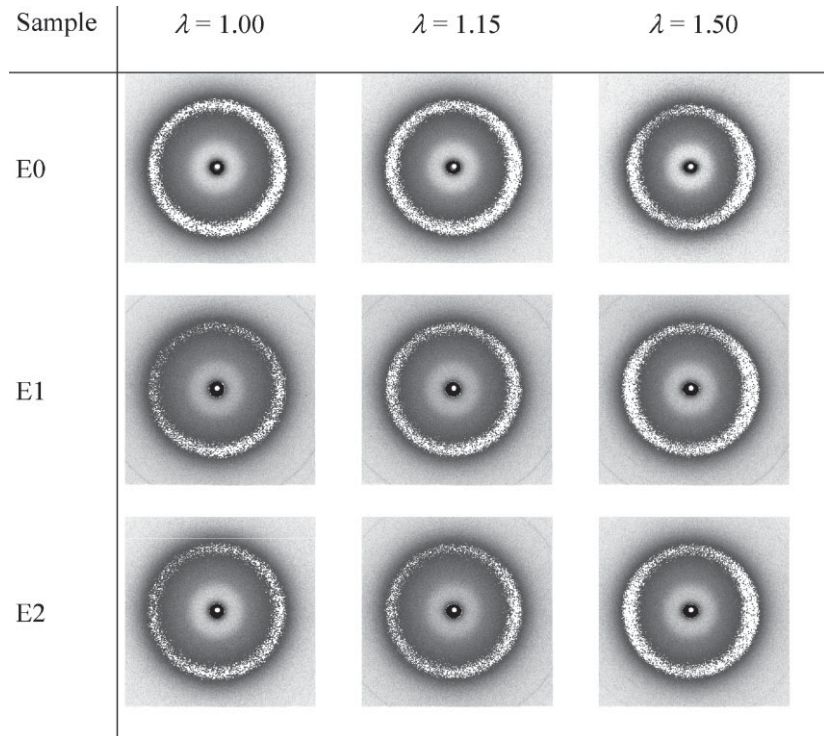


Figure 4. 2D WAXS patterns for the three elastomeric samples E0, E1, and E2 at the strain values of $\lambda = 1.0$, 1.15 , and 1.50 .

Furthermore, the presence of both kinds of nanoparticle makes the elastomer more brittle as can be observed by the maximum elongation during deformation. The pure reference system (E0) could be drawn up to strain values of $\lambda_{\max}=2.83$, while for the nanocomposites only values of $\lambda_{\max}=1.48$ for E1 and $\lambda_{\max}=1.56$ for E2 were obtained. The toughness, i.e., energy applied until rupture of the sample, of the reference elastomer ($5.7 \text{ J} \cdot \text{cm}^{-3}$) differs considerably (800%) with respect to the values for both IOENs ($0.6 \text{ J} \cdot \text{cm}^{-3}$). This indicates that the nanoparticles act as defects for crack initiation, reducing the toughness of the elastomeric matrix.

In order to evaluate and compare the efficiency and energy needed during the deformation process for the three samples, the area under each stress/strain curve at fixed strain was calculated. The energy at $\lambda = 1.48$, the maximum elongation for sample E1, shows noticeable differences between the samples. The energy for the sample with FNPs (E1) is 32% higher than for the reference sample (E0), whereas for the sample with NPs (E2) it is only 6%, providing further evidence for mechanical enhancement of the crosslinkable nanoparticles in the nanocomposite. In Table 1, the Young's modulus (E), maximum strain (λ_{\max}), energy at $\lambda = 1.48$ (U), and toughness (U_{\max}) for the three elastomeric samples are summarized.

Mechanical Coupling between Polymers and Nanoparticles

The next point assessed is whether any coupling between the polymer matrix and the nanoparticles exists, that is, if the external mechanical field which orients the polymer backbones induces any kind of alignment to the nanoparticles. In order to observe any potential effect, both nanocomposites (E1 and E2) as well as the reference elastomer E0 were analyzed by SAXS (in the region where the nanoparticles diffuse, $0.055 \text{ nm}^{-1} < q_{\text{FNP}} - q_{\text{NP}} < 0.15 \text{ nm}^{-1}$) and by WAXS experiments (where the polymer chains interact and align, $6.0 \text{ nm}^{-1} < q_{\text{PC}} < 20 \text{ nm}^{-1}$) during the stretching process.

In the WAXS region (Figure 3a), the elastomeric matrix already shows

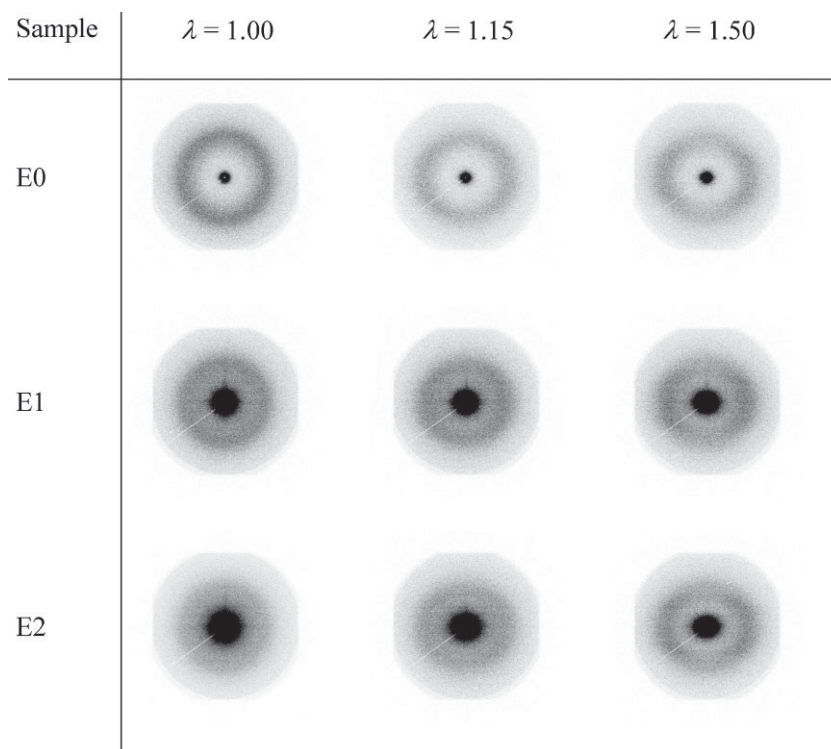


Figure 5. 2D SAXS patterns for the three elastomeric samples E0, E1, and E2 at the strain values of $\lambda = 1.0$, 1.15 and 1.50 .

scattering peaks at $q_{\text{PC}} = 14.4 \text{ nm}^{-1}$ ($d_{\text{PC}} = 0.44 \text{ nm}$) and $q_{\text{MPS}} = 1.20 \text{ nm}^{-1}$ ($d_{\text{MPS}} = 5.2 \text{ nm}$). The first peak q_{PC} is related to the polymer backbone chains distance. The second peak q_{MPS} is the disordered microphase separated domains between the aliphatic segments of the crosslinker and the ether segments of the polymer chains. This second scattering peak is enhanced by the presence of hydrogen

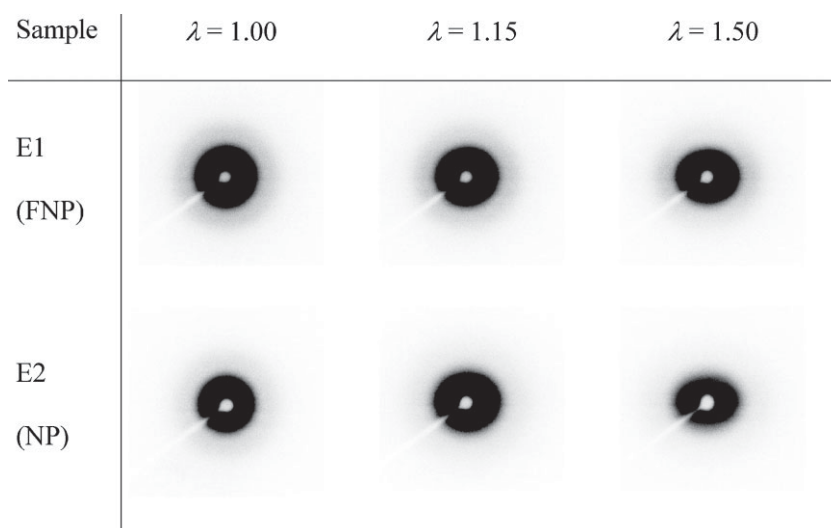


Figure 6. 2D SAXS patterns of the nanoparticles (FNP and NP) at the strain values of $\lambda = 1.0$, 1.15 and 1.50 .

bonding of the urea motifs created during the condensation polymerization process.^[22] The two IOEN samples also show scattering peaks at $q_H = 16.9, 23.1$, and 24.8 nm^{-1} , which correspond to the $\alpha\text{-Fe}_2\text{O}_3$ nanoparticles in their hematite form.

In the SAXS region (Figure 3b), the two IOEN samples show two scattering peaks related to the anisotropic shape of the ellipsoidal SCH nanoparticles. The peaks q_{FNPa} and q_{NPb} correspond to the long a -axis of the nanoparticles, and the peaks q_{FNPb} and q_{NPb} to the b -axis. The FNPs have lower peak values, i.e., greater distances, for both axes with respect to the NPs. This difference is attributable to the layer thickness which contains the PVP and silica layer, plus the functional groups that reacted with the polymer matrix.

Experiments were carried out at strain values of $\lambda = 1.00, 1.15$, and 1.50 (Figure 4 and 5). Already the 2D scattering patterns show insightful information for both samples: i) the samples are becoming aligned upon stretching in the same direction parallel to the applied stress and ii) the intensity of the crosslinkable nanoparticles is much higher than the non-crosslinkable ones (Figure 6). This can be easily explained by the better dispersion achievable with FNPs with respect to NPs, which exhibit a higher tendency to aggregate, as shown in our previous work.^[3]

The azimuthal Gaussian distribution of all scattering peaks ($q_{\text{PC}}, q_{\text{MPS}}, q_{\text{FNPb}}$, and q_{FNPa}) allows evaluation of the order in the sample in terms of the polymer matrix and the nanoparticles (Figure 7). The orientational order parameter S is calculated based on the average of the second Legendre polynomial according to the literature^[26,27] from the azimuthal scattering intensity distribution $I(\varphi)$ as:

$$S = -2P_2 = -2 \left\langle \frac{3\cos^2\varphi - 1}{2} \right\rangle$$

$$= - \frac{\int_0^{\pi/2} I(\varphi)(3\cos^2\varphi - 1)\sin\varphi d\varphi}{\int_0^{\pi/2} I(\varphi)\sin\varphi d\varphi} \quad (1)$$

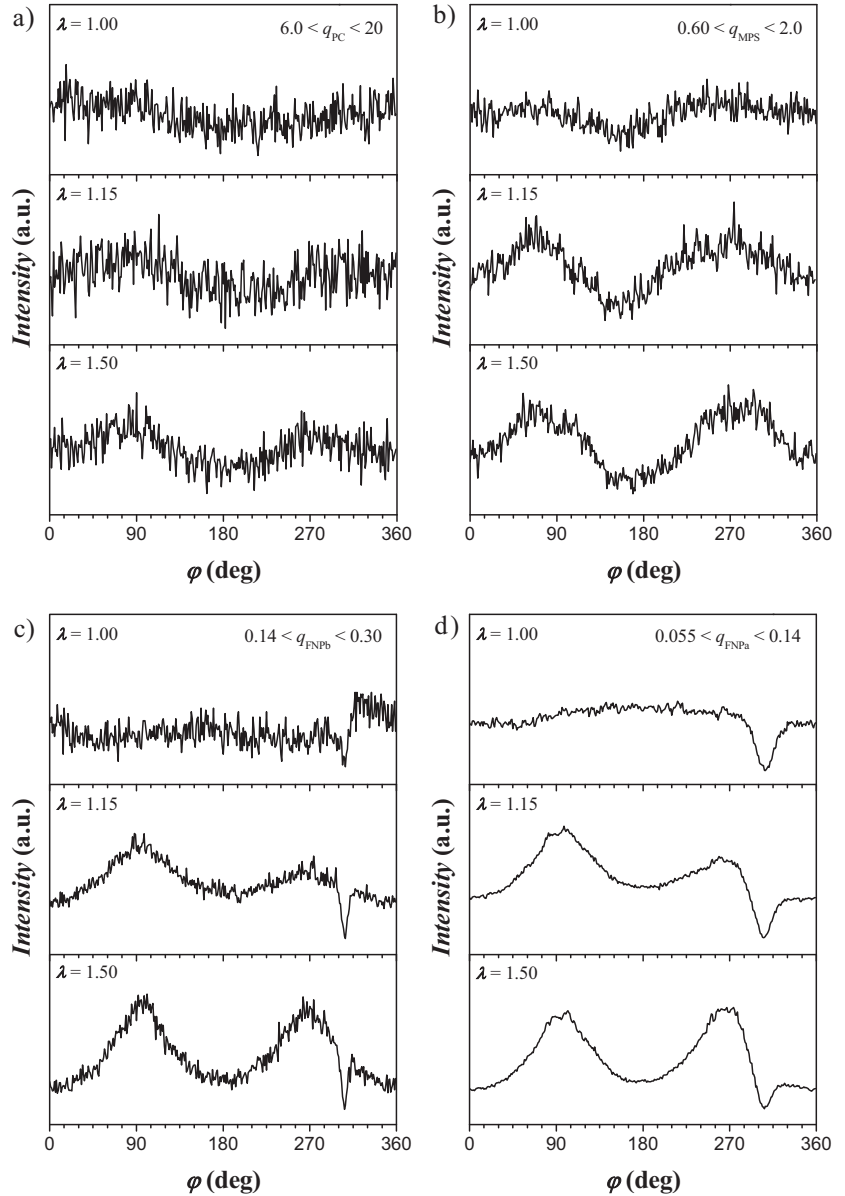


Figure 7. Azimuthal scattering distributions of the sample E1 at a) $6.0 \text{ nm}^{-1} < q_{\text{PC}} < 20 \text{ nm}^{-1}$, b) $0.60 \text{ nm}^{-1} < q_{\text{MPS}} < 2.0$, c) $0.14 \text{ nm}^{-1} < q_{\text{FNPb}} < 0.30 \text{ nm}^{-1}$, and d) $0.055 \text{ nm}^{-1} < q_{\text{FNPa}} < 0.14 \text{ nm}^{-1}$ at the strain values of $\lambda = 1.00, 1.15$ and 1.50 .

In Figure 8, the evolution of the orientational order parameters as a function of the applied strain is presented for the three elastomeric samples at the different scattering regions. The orientational order parameter of the polymer chains (Figure 8a) goes up to $S = 0.33, 0.24$, and 0.31 , and the orientational order parameter of the micro-phase separated domains (Figure 8b) up to $S = 0.35, 0.37$, and 0.35 for the samples E0, E1, and E2, respectively, when the strain reaches $\lambda = 1.50$. The orientational order parameter for the nanoparticles (Figure 8c and 8d) increases faster than the previous ones when stretching the samples, reaching values of $S = 0.50\text{--}0.51$ and $0.56\text{--}0.53$ for the two IOEN

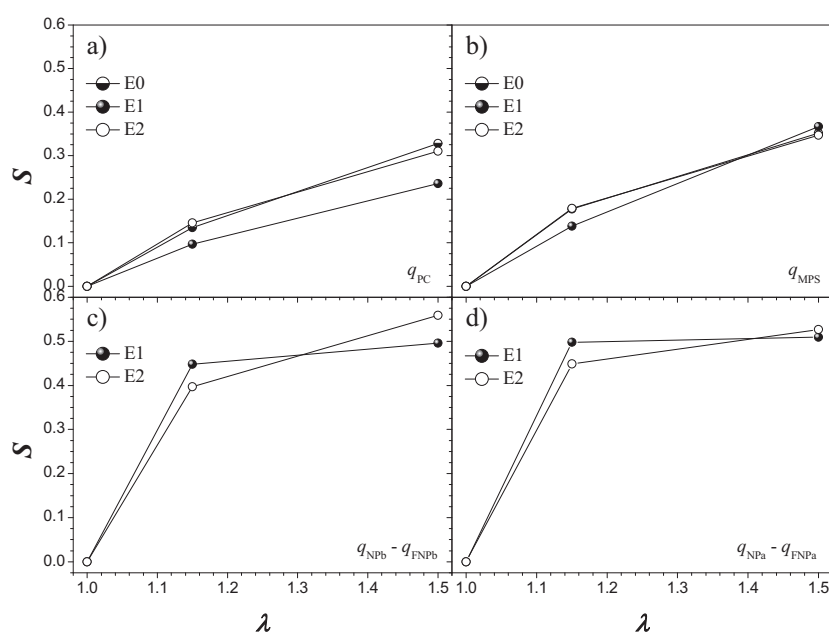


Figure 8. Order parameter (S) as a function of the strain (λ) for the three elastomeric samples at a) $6.0 \text{ nm}^{-1} < q_{PC} < 20 \text{ nm}^{-1}$, b) $0.60 \text{ nm}^{-1} < q_{MPS} < 2.0$, c) $0.14 \text{ nm}^{-1} < q_{NPb} < 0.30\text{--}0.16 \text{ nm}^{-1} < q_{NPb} < 0.33 \text{ nm}^{-1}$, and d) $0.055 \text{ nm}^{-1} < q_{NPb} < 0.14\text{--}0.055 \text{ nm}^{-1} < q_{NPb} < 0.16 \text{ nm}^{-1}$.

samples E1 and E2, respectively. It seems that less stretching is needed for the orientation of the nanoparticles compared with both the inter-chain and inter-domains distances.

By analyzing the azimuthal distribution of the scattering intensities at different strain values for both IOEN samples, it is apparent that they essentially align in an identical way irrespective of their chemical (E1) or physical (E2) adhesion to the polymer matrix. Thus, it can be inferred that large nanoparticles such as those used in the present study are fully coupled to the polymer network and any deformation in the elastomeric matrix induces and controls their alignment and the resulting mechanical properties.

Conclusion

We have demonstrated the physical interactions between nanoparticles and the polymer matrix in a hybrid nanocomposite formed by an elastomeric matrix loaded with ellipsoidal SCH nanoparticles. An increase of 20% for the Young's modulus was demonstrated from the integration of 0.5 wt.% ellipsoidal nanoparticles acting as cross-linking agents. At an equivalent concentration, surface-untreated nanoparticles were found to act as defects, and the Young's modulus of their corresponding elastomer was barely increased with respect to the reference sample. Both nanocomposites exhibited increased brittleness as compared to the reference matrix, as a consequence of

nanoparticle-induced fracture initiation: this resulted in a maximum achievable deformation of 50% ($\lambda = 1.50$) prior to fracture.

Evidence of the strain-induced orientation of the ellipsoidal-shaped nanoparticles was provided by the SAXS pattern of the nanocomposite under mechanical stress. Independent of the type of interaction between the nanoparticles and the elastomeric matrix, coupling between the polymer network and the nanoparticles was confirmed, as shown by the values of their orientational order parameters.

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Keywords: elastomers; hematite nanoparticles; nanocomposites; stress/strain; X-ray scattering

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